

Spectrophotometric and nephelometric detection unit

5 The present invention relates to a method and an apparatus for the essentially simultaneous performance of spectrophotometric and nephelometric analyses principally in in-vitro diagnosis.

10 While on the one hand an increasing demand for more sensitive optical detection methods for automated in-vitro laboratory analysis has evolved in recent years, at the same time requirements for increasing alignment and harmonization of the analytical methods have been
15 instituted.

These requirements can be comprehended against the background of the concentration of the number of measurement laboratories in the form of a few centers
20 for laboratory diagnosis. Only by more extensively matching the analytical methods and reducing the number of different equipment variants or method conditions can the tests be carried out simply and without increased operational requirements. These endeavors are
25 thereby intended to result in further cost savings in the field of diagnosis.

The need for more complex, fully automated analysis equipment is growing at the same time. In order to be
30 able to process a multiplicity of different samples and types of samples and to achieve the required throughput, said analysis equipment is additionally coupled via corresponding networks to laboratory integration systems for discontinuous tracking of
35 sample, test or consumable material.

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Capital expenditure and subsequent capacity utilization of such fully automated analysis machines can only be achieved, however, if at the same time there is also harmonization in analysis in the different fields of application of in-vitro diagnosis. Thus, even now, attempts are being made to implement inter alia parameters of clinical chemistry, plasma protein diagnosis or immunochemical diagnosis on common platforms. This is successful particularly when the requirements made of the process technology in the different fields of application are similar. This is because the conditions for the treatment of samples or of reagents solutions with regard to storage (temperature stability) or metering (volume, precision) often correspond well.

Thus, the increasing matching and harmonization should also consistently extend to the detection methods used for analysis.

Most of the analytical methods employed at the present time only use a way of obtaining measurement data of the kind offered by photometry or light scattering. In certain analysis methods, the light scattering is detected at different angles or under different angular ranges. Scattered-light methods are extremely sensitive and their resolution is superior to that of photometric methods particularly for methods in which the formation and temporal change of scattering centers are detected, as is the case in agglutination tests or in methods of particle-enhanced in-vitro diagnosis. Comprehensive considerations and calculations concerning the theory of scattered light are adequately known per se to the person skilled in the art and are textbook material (thus, for example, C.F. Bohren, D.R. Huffman, Absorption and Scattering of Light by Small Particles, J. Wiley & Sons, 1983). Further aspects of application to in-vitro diagnosis tests may be found inter alia in E.P. Diamandis et al. 1997 (Immunoassay, Academic

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Press, 1997, Chapter 17: Nephelometric and Turbidimetric Immunoassay) and the references cited therein.

5 On the other hand, the requirement for many test
methods consists ^{of} ~~in~~ carrying out photometric tests
which purely detect absorption. The scattered-light
signal fails in these cases since, at best, the
contaminants contained in the material to be measured
10 can be measured.

By way of example, DE-A 2409273 and US patent 4,408,880
describe methods in which a sample is excited by a
laser beam and its scattered light is detected at an
15 angle outside the beam axis of the incident light. The
scattered light used for the measurement is masked out
by a suitably shaped annular diaphragm which retains
the excitation light from the laser.

20 US patent 4,053,229 likewise describes an apparatus for
measuring scattered light, in which a scattered light
measurement is effected simultaneously at an angle of
2° and at an angle of 90°.

25 WO 98/00701 describes a combination of a nephelometer
with a turbidimeter which comprises two light sources.
While one of these, in the form of a laser, produces
the scattered light which is detected at 90°, a diode
(LED) emitting in the infrared spectral region serves
30 for measuring the turbidity on the axis of the incident
light. The method described in the application serves
in particular for improved control of the intensity of
the laser used.

35 To date, there are no known methods and/or apparatuses
which enable both scattered-light measurements and
photometric measurements to be carried out essentially
simultaneously.

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B Note

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Light from one ~~One~~ or more

~~sources 1, 2 are guided via a common beam guidance arrangement 24 to the reaction location 11. Scattered~~

a spectrophotometer

While nephelometry is used predominantly for the analysis of agglutination tests and in particle-enhanced immunodiagnosis, photometry serves for measuring numerous other clinical-chemical parameters

based on spectral changes. The combination makes it possible to achieve the aim of being able to carry out a multiplicity of different diagnostic tests pertaining to clinical chemistry, immunodiagnosis, plasma protein
5 diagnosis or coagulation diagnosis on a single module.

The present description relates to the field of the use of automated measurement systems in analysis and in in-vitro diagnosis. In particular, the apparatus described
10 makes it possible to simultaneously carry out tests which are measured with the aid of scattered-light measurement and/or by photometry in the UV-Vis spectral region.

15 In particular, the unit can be integrated in systems in which the measurement of a multiplicity of samples and tests in measurement cuvettes is carried out on a common rotor or carousel, as is often the case for automatic analysis systems.

20 The invention has developed an apparatus which makes it possible to measure both the scattered light from a sample, which is produced at angles outside the axis of the incident light, and the light transmitted at angles
25 around 0° .

Different narrowband or broadband light sources can be used to excite the material to be measured. These are guided on a common beam guidance arrangement to the
30 reaction location. The pulsed driving of the light sources enables mutual disturbances or interference to be completely suppressed.

It is likewise an aim of the method described to carry
35 out a validation of the beam path and the components used, such as the light source, the optical components of lenses and diaphragms and the properties brought about by the moving accommodating vessels of the material to be measured (cuvettes).

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The method according to the invention and an apparatus are explained in more detail below by way of example using just one embodiment.

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Fig. 1 schematically shows an arrangement of light sources 1, 2, ^{reaction location} ~~receptacle~~ 11 for material to be measured (cuvette) and detectors 17, 22, 25. As is evident from

10 this, solid angles around the axis of the incident light are utilized in both methods. In the arrangement used most for scattered-light measurement, the scattered light is detected at an angle of 90°. Separation of the incident light from the scattered light is particularly easy to achieve as a result. On
15 the other hand, choosing a larger solid-angle range and utilizing angles or angular ranges around the forward direction of the incident light make it possible to achieve higher intensities of the scattered light, as a result of which an arrangement can be constructed in a
20 technically simple and more cost-effective manner. The proportion of scattered light at angles around the forward direction is particularly high precisely for the measurements (which are striven for in accordance with the present description) on organic macromolecules
25 with utilization of a particle-enhanced immunoassay for use in human in-vitro diagnosis.

The light sources 1, 2 employed for the analysis have different spectral bandwidths in accordance with the
30 application which is striven for. While a light source for the scattered-light measurement has a narrowband emission in the red or infrared spectral region, preferably in the range between ⁶⁰⁰ ~~650~~ and 950 nm, the light source for photometric measurements typically
35 emits in a spectral region between 300 and 800 nm. Both light sources are used in pulsed operation in the present embodiment.

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For the purpose of common beam guidance and excitation of the measurement cuvette, the light from both sources is guided to a coupling unit 4 for example via optical waveguides or bundles of fibers and is coupled out via suitable optical components. A dichroic beam splitter 5 specifically adapted for the two bandwidths enables both light sources to be guided on the common beam axis 24. Corresponding lenses 6, 9 are used to collimate the beam for the later measurement. A fraction of the incident lights can be masked out, by means of a further beam splitter 8, for the reference measurement

22, 23

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following the common beam axis

The light beam 24 impinging through a diaphragm 10 on the material 12 to be measured which is situated in a reaction location cuvette 11 leads to scattering or absorption, depending on the type of material to be measured.

However, the pulsed excitation of the two light sources means that both methods can be carried out independently of one another. The information which is necessary for triggering one of the light sources can in this case be chosen by way of a test definition, which is necessary prior to the measurement, and is thus known to the system while the measurement is being carried out.

The physical separation of the axially transmitted and of the scattered light 20 is effected by a diaphragm 13 arranged on the beam axis. In this case, the diaphragm is advantageously configured in such a way that it serves on the one hand as a scattered light trap and on the other hand as a deflection unit for the axially incident light. To that end, the diaphragm is constructed as an annular and perforated diaphragm. By the choice of an internal and external diameter, it is possible to select the most favorable solid-angle range for the analysis. The proportion which is transmitted as scattered light through the diaphragm is focused

onto the input of a detector 17 by means of a lens or a lens system 14.

While the scattered light measurement usually involves a discrete, narrowband wavelength, a broader-band light source is used for the photometric measurement, with the result that the signal used for a photometric measurement should be evaluated further. For this purpose, the light impinging on the beam axis around 0° is coupled out with the aid of the diaphragm 13, the central part of which is designed as a perforated diaphragm. The latter preferably has a diameter of from 0.5 to 3 mm, which limits the incident beam cross-section. In this case, the beam can be deflected by a prism 18 or another suitable light guidance system, such as a correspondingly curved bundle of fibers, for example. The light is coupled into the bundle 19 of fibers by means of the optical components known to the person skilled in the art. The bundle of fibers subsequently serves as entrance slit of a spectrophotometer 25. In this case, the known principle of a diode linear array is used as the spectrophotometer, and, equipped with no mechanical components, allows a short measurement time with a full spectral bandwidth.

After the signal has been evaluated and the spectrum $i=f(\lambda)$ has been obtained, the data are fed to a computer 27 for further processing.

According to the invention, the arrangement described is frequently employed in analysis systems in which, for an increased throughput, a multiplicity of measurement cuvettes are to be processed simultaneously. For this purpose, the cuvettes ~~11~~ are positioned on a rotatable carousel or rotor, as evident from Fig. 3, for example. This likewise clarifies the favorable mode of use of the pulsed operation in accordance with Fig. 2: if a ~~cuvette~~ ^{reaction location} 11 is situated in

the region 32, 34 which is accessible to the measurement optics within a time interval $\Delta 1$, a pulse ($\Delta 2$) from one of the available light sources 1, 2 can be triggered, and is applied to the ~~cuvette 13 via 33~~ and the coupling unit 32. The signal obtained from this is detected within the time interval $\Delta 4$. Depending on the type of test and associated evaluation method, the transmitted or scattered proportion of the light is detected by the sensors 17 and 22, respectively. The type of driving thus permits completely separate excitation of the material to be measured by the different light sources and exhibits no mutual influencing of the scattered or of the transmitted light. An additional time interval $\Delta 3$ illustrated in Fig. 2 serves for the possible detection of a reference signal by sensor 17 and 22 for the adjustment of a dark value.

By cyclically rotating a carousel 31 equipped with cuvettes, it is possible to measure a subsequent cuvette.

In addition to these two primary methods, a host of possibilities may be opened up in which the two methods complement one another:

1. Calibration of the light source by the spectrophotometer 25: the momentary introduction of a standard 7 into the beam path can be used for determination of the wavelengths or absorption.

2. Testing the positioning of a cuvette situated in the region of the measurement unit: cyclic movement of a cuvette situated on the rotor enables the recording of a location-dependent cuvette profile and the further position determination thereof.

3. Fluorescence/chemiluminescence mode: a material 12 to be measured which is situated in the cuvette 11 can

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be selectively excited by means of one of the light sources 1, 2, if appropriate with the utilization of further filters 7. By means of the detector 17, the resulting fluorescent light can be detected, under
5 certain circumstances by the use of further blocking filters 15.

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Description of the Figures

Fig. 1 shows a schematic overview of an embodiment of the analysis unit which is described in more detail
5 below.

Fig. 2 represents a timing diagram of the driving of the different light sources and the recording of measured values.

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Fig. 3 shows the use of the measurement unit within a rotatable rotor for accommodating a multiplicity of measurement cuvettes arranged in a circle.

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List of reference symbols for the figures:

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| 1. Light source 1 | 19. Bundle of fibers/
optical waveguides |
| 2. Light source 2 | |
| 3. Light guidance arrangement
(bundle of fibers) | 20. Light emerging from
cuvette |
| 4. Coupling unit | 21. Scattered light |
| 5. Beam splitter (dichroic) | 22. Sensor for reference
measurement |
| 6. Lens system/lens 1 | 23. A/D converter |
| 7. Filter | 24. Common beam axis |
| 8. Beam splitter | 25. Spectrophotometer |
| 9. Lens system/lens 2 | 26. A/D converter |
| 10. Diaphragm | 27. Computer |
| 11. Cuvette/reaction location | 28. Screen |
| 12. Material to be measured | 29. Keyboard |
| 13. Diaphragm | 30. Cuvette/reaction
location |
| 14. Lens system/lens | 31. Carousel/rotor for
accommodating cuvettes |
| 15. Blocking filter | 32. Illumination unit with
optical waveguide coup-
ling in arrangement |
| 16. Diaphragm | 33. Beam guidance arrange-
ment |
| 17. Sensor/detector | 34. Detection unit |
| 18. Beam deflection arrangement
(e.g. prism) | |

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